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Micro-macro models for reactive transport in elastically deformable biological tissue

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Motivation

Describe reactive transport of nutrients, drugs, respiratory gases or waste products through deformable tissues such as lung tissue,



- heart tissue or vessel walls.
- Cellular structure leads to multi-scale character of biological tissue
- Diseases like Cancer, Covid-19 or Sepsis lead to **impairment of cellular** reaction networks (e.g. energy metabolism)
- *Lung-on-a-chip*: a microdevice illustrates effect of **cyclic stretching** on transport processes in deforming bio-engineered lung tissue



Multi-Scale Modeling

System of linear elasticity and reactive transport in mixed Eulerian/Lagrangian framework on the periodic microscopic domain:

 $\text{in } (0,T) \times \varOmega_{\varepsilon}^{\mathbf{s}},$ $\varepsilon^2 \partial_{tt} \mathbf{u}_{\varepsilon} - \nabla \cdot (\mathbf{Ae}(\mathbf{u}_{\varepsilon})) = \mathbf{f}_e$ $\partial_t \widehat{c}_{\varepsilon} + \widehat{\nabla} \cdot \left(\widehat{\mathbf{v}}_{\varepsilon} \widehat{c}_{\varepsilon} - \widehat{\mathbf{D}}^m \widehat{\nabla} \widehat{c}_{\varepsilon} \right) = f_d^m (\widehat{\mathbf{c}}_{\varepsilon}) \quad \text{in } \cup_{t \in (0,T)} \{t\} \times \Omega_{\varepsilon}^{\mathbf{s}}(t),$

Numerical Justification of the Effective Model

Use feed-forward neural network

to compute effective coefficients

700 times faster

Is the effective micro-macro model a good approximation of the microscopic model?



with unknown deformation S_{ε} :

 $\mathbf{S}_{\varepsilon}(t,x) := x + \mathbf{u}_{\varepsilon}(t,x),$

and current deformed domain $\Omega_{\varepsilon}^{s}(t)$: $\Omega_{\varepsilon}^{\mathbf{s}}(t) := \{ \widehat{x} \in \mathbb{R}^n \mid \widehat{x} = \mathbf{S}_{\varepsilon}(t, x), \ x \in \Omega_{\varepsilon}^{\mathbf{s}} \}.$



• **Pull-back** of the transport problem using the deformation \mathbf{S}_{ε} to obtain a microscopic model in **unified** *Lagrangian* framework with

$c_{\varepsilon}(t,x) := \widehat{c}_{\varepsilon}(t,\mathbf{S}_{\varepsilon}(t,x)).$

• **Upscale** transformed problem using the method of **two-scale** asymptotic expansions to obtain an effective micro-macro **model** in the homogeneous domain Ω :

> $-\nabla \cdot (\mathbf{A}^* \mathbf{e}(\mathbf{u}_0)) = |Y^s| \mathbf{f}_e$ in $(0,T) \times \Omega$, in $(0,T) \times \Omega$. $\partial_t \left(J^* c_0 \right) - \nabla \cdot \left(\mathbf{D}^* \nabla c_0 \right) = J^* f_d(c_0)$

- The system is nonlinearly coupled via effective coefficients A^*, J^* and D^* , which are obtained by means of auxiliary **cell problems** on the fixed reference cell Y^s , e.g.

Simulation Results

Time-evolution of concentration while domain is under cyclic elastic deformation, mimicking e.g. the **breathing movement**:





References

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